

Spatial and temporal skin blood volume and saturation estimation using a multispectral snapshot imaging camera

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Background

- The oxygenation of living tissue is a fundamental parameter to for the homeostasis of cells, tissue and organs.
- Microcirculation of tissue is spatial and temporal heterogeneous.
- Clinically, visual observations of temporal and spatial skin colour variations, as a reaction to provocation, can be used to indirectly assess the microcirculatory blood perfusion and oxygenation.

Background

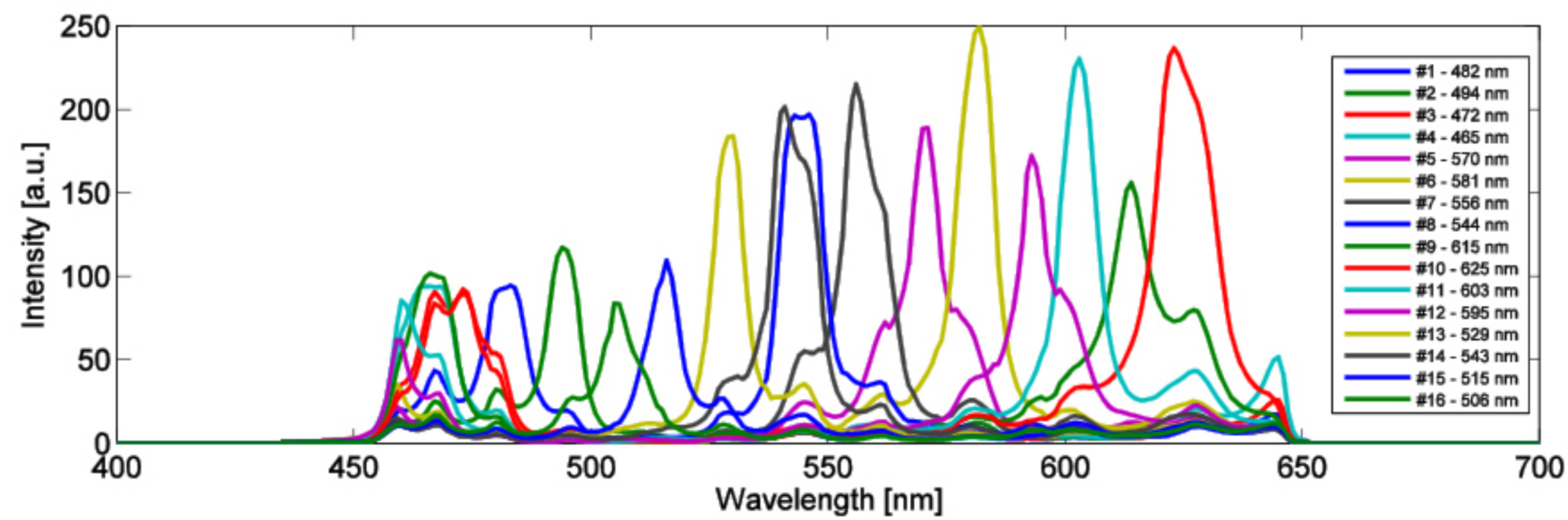
- Standard diffuse reflectance spectroscopy utilize optical fiber probes with a well-defined distance between sending and receiving fibers.
- Hyperspectral imaging combine spectroscopy and imaging techniques to acquire spectral and spatial information.
 - Manual mapping
 - Monochrome camera with LCTF or optoacoustic filters or
 - Hyper- or Multi-spectral cameras

Aim

- Evaluate a multispectral snapshot imaging system to estimate skin blood volume and oxygen saturation with high temporal and spatial resolution

xiSpec camera

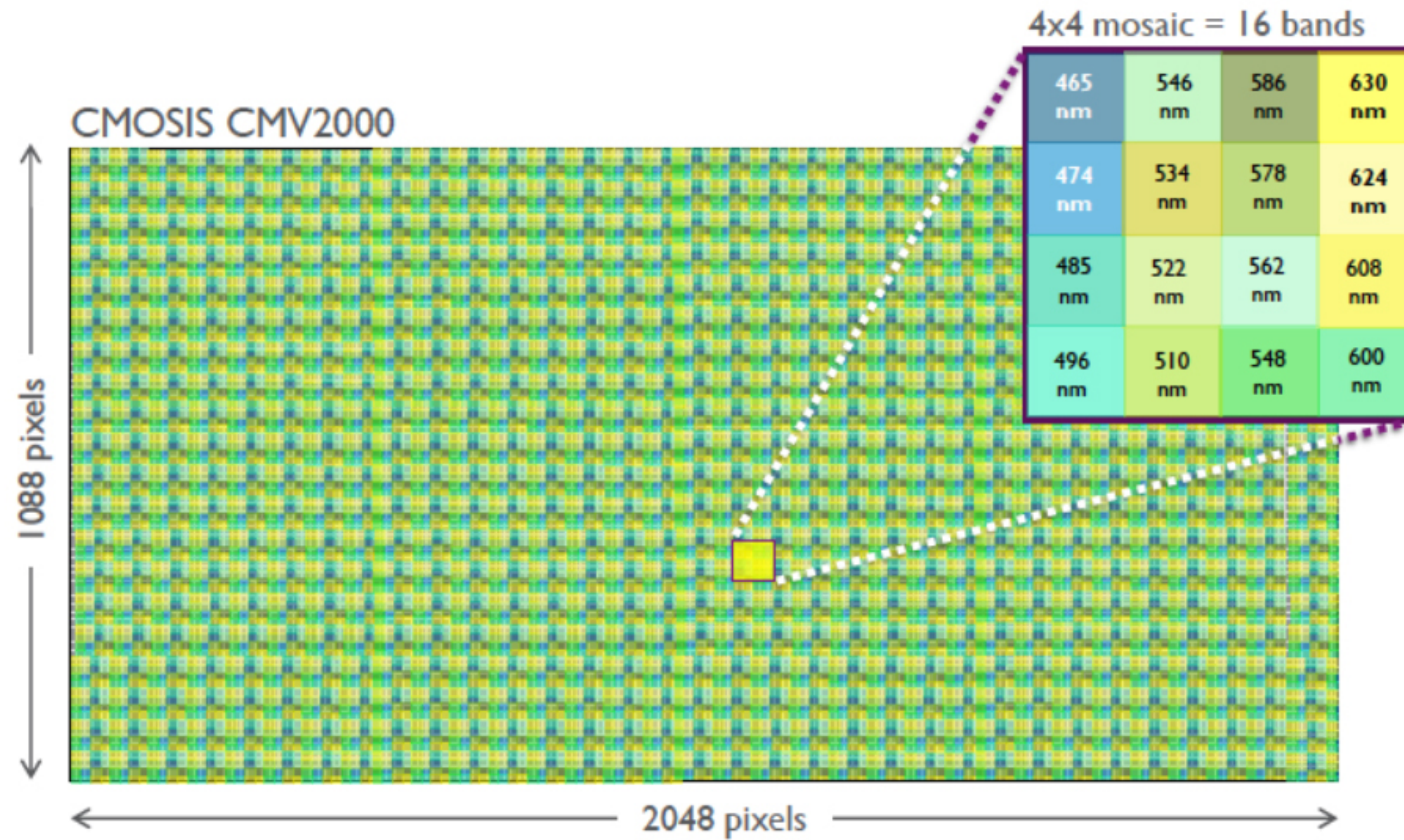
- MQ022HG-IM-SM4X4-VIS, XIMEA®
 - 4x4 mosaic detector (CMOS)
 - 16 wavelength bands (465-630 nm)
 - Image size: 512 x 272 (per band)
 - FPS: 170 data-cubes/s



SNAPSHOT MOSAIC HSI SENSOR (GENI)

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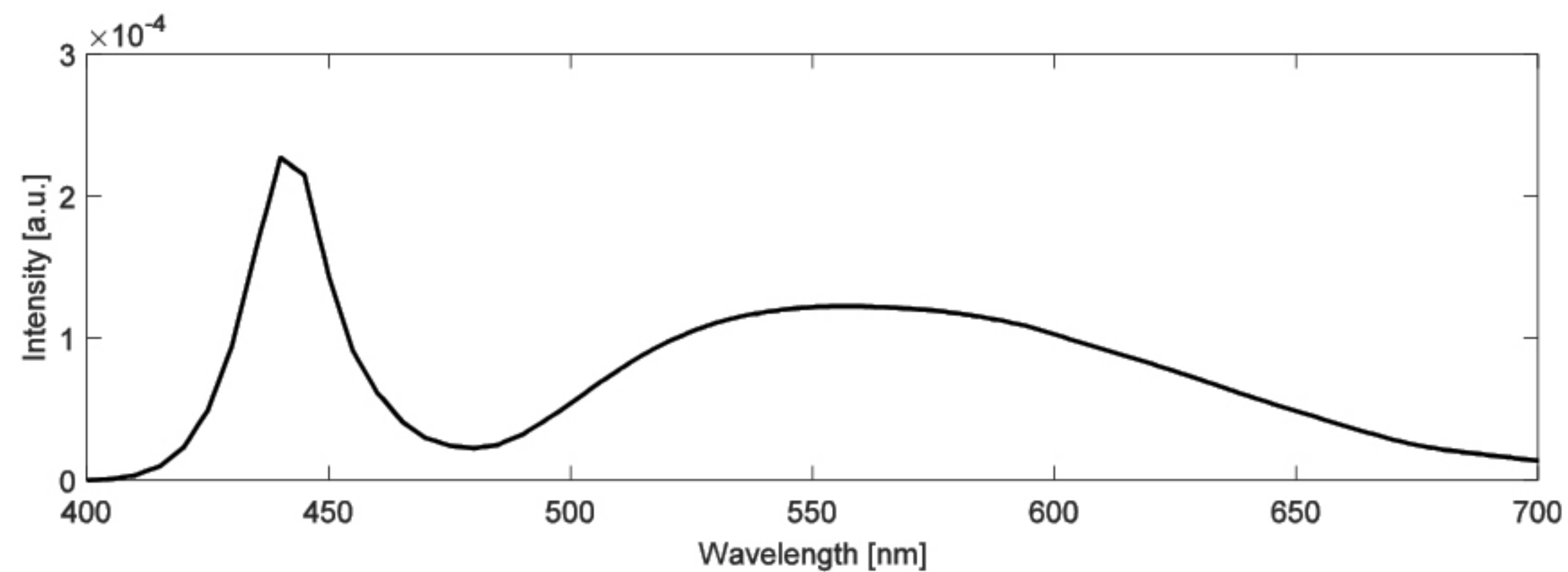
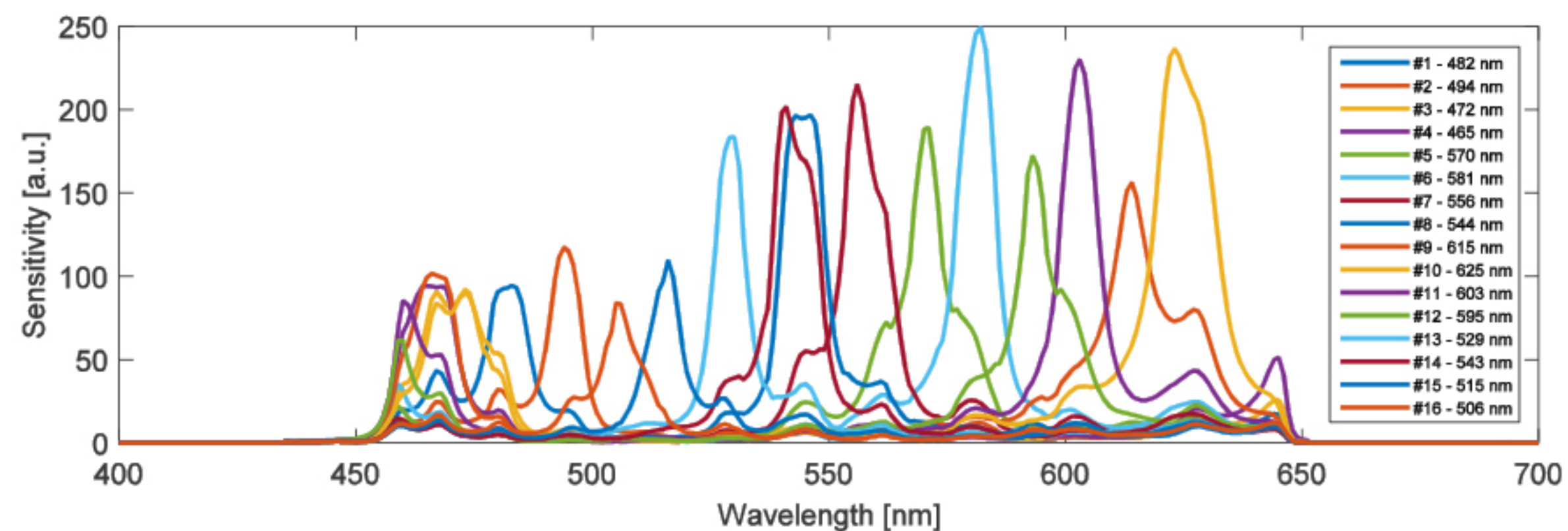


■ Key specifications

- **Spectral resolution:** 4x4 mosaic (1 filter / pixel) = 16 bands in 470-630nm
- **FWHM:** ~ 15nm
- **Spatial resolution:** from 512x272 (RAW per band)
- **Speed:** up to 340 data-cubes / s (max sensor limit)

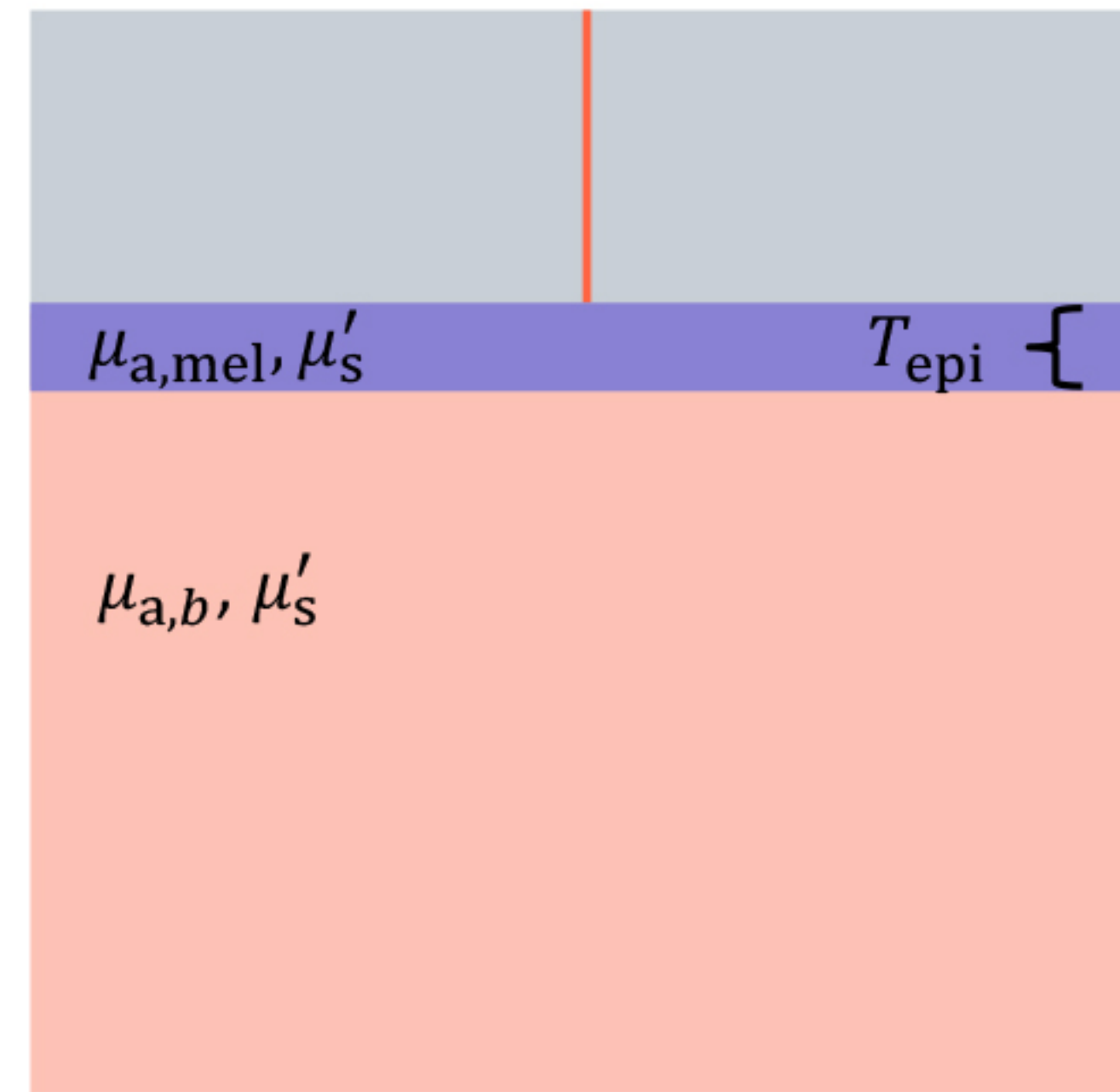
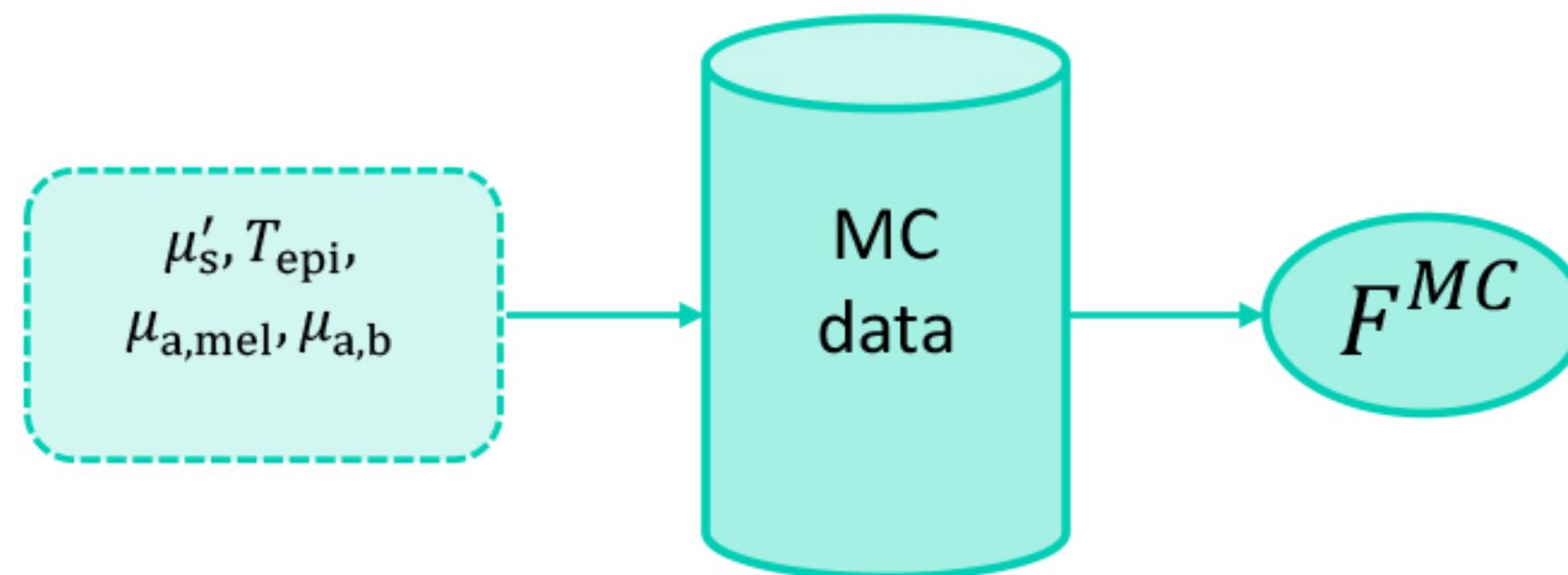


Modelling detected light



Forward Monte Carlo model

- Monte Carlo simulations to create a look-up table
 - Two-layered tissue model
 - Discrete values of μ'_s , T_{epi} , $\mu_{a,\text{mel}}$ and $\mu_{a,b}$ relevant to human skin



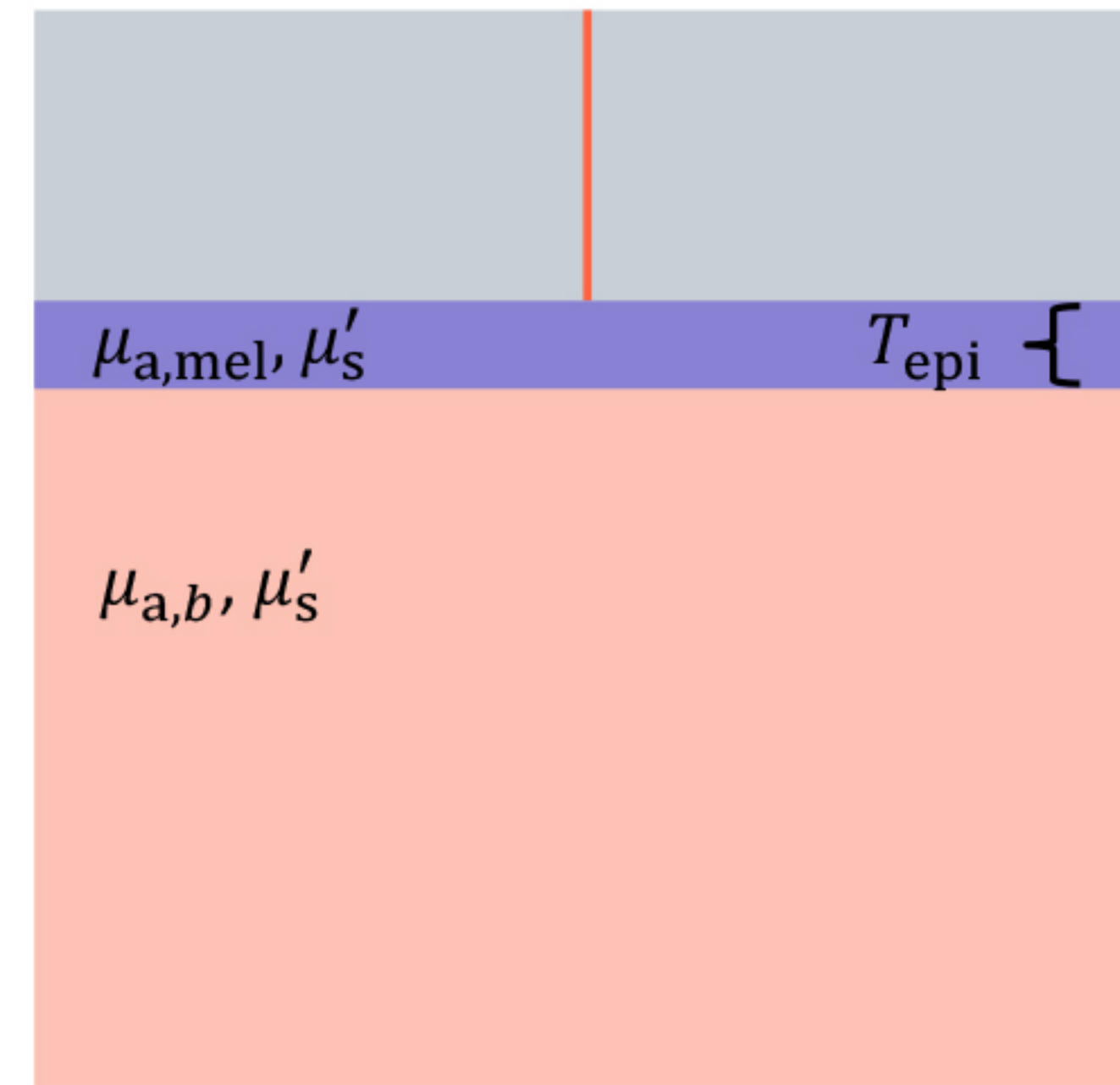
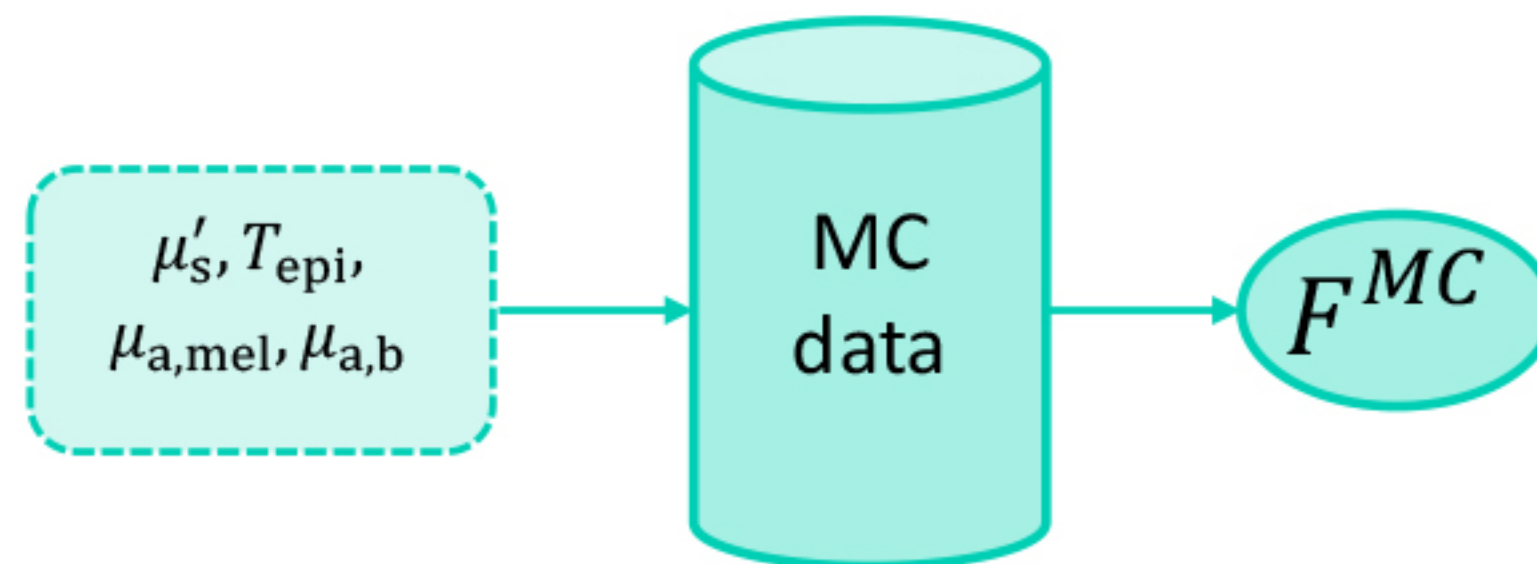
Forward Monte Carlo model

- Monte Carlo simulations to create a look-up table

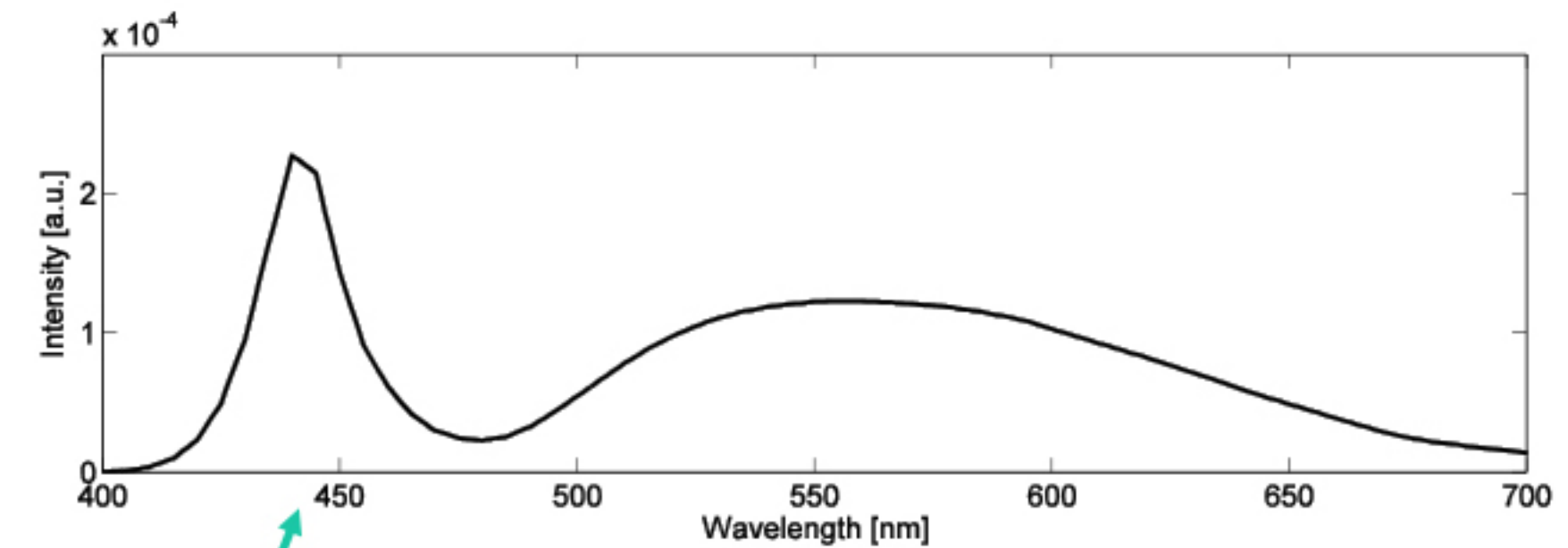
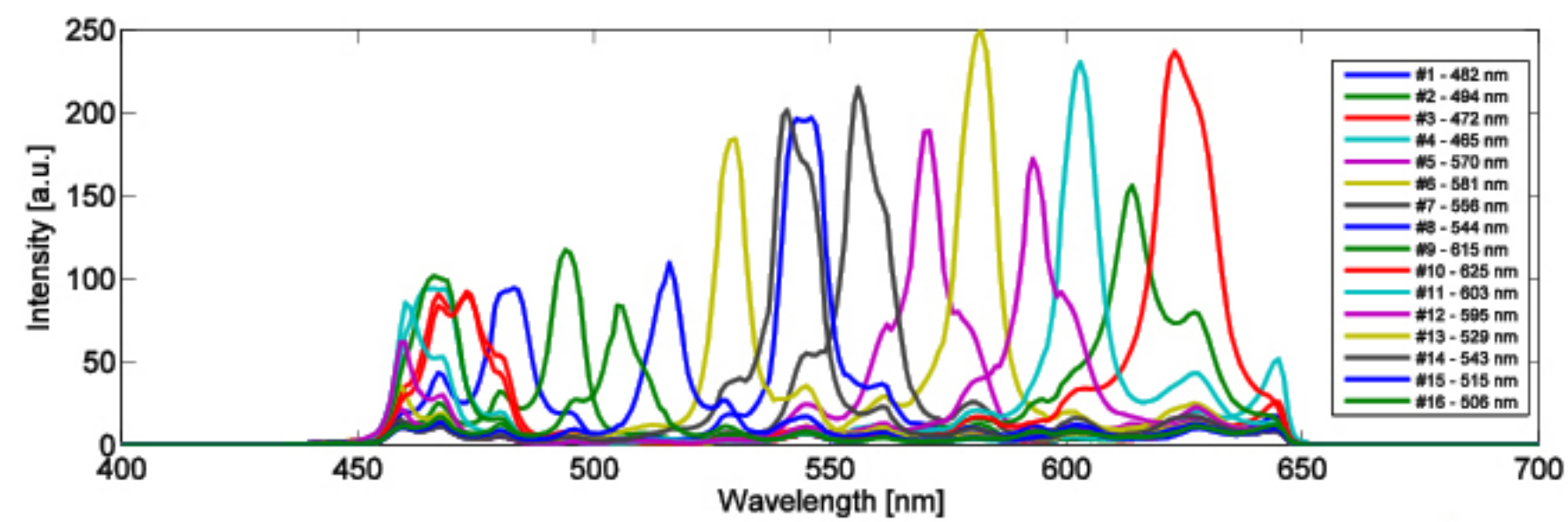
$$\mu'_s(\lambda) = \alpha \cdot \left(\frac{\lambda}{500}\right)^{-\beta}$$

$$\mu_{a,\text{mel}}(\lambda) = c_{\text{mel}} \cdot 51.9 \cdot \left(\frac{\lambda}{500}\right)^{-3}$$

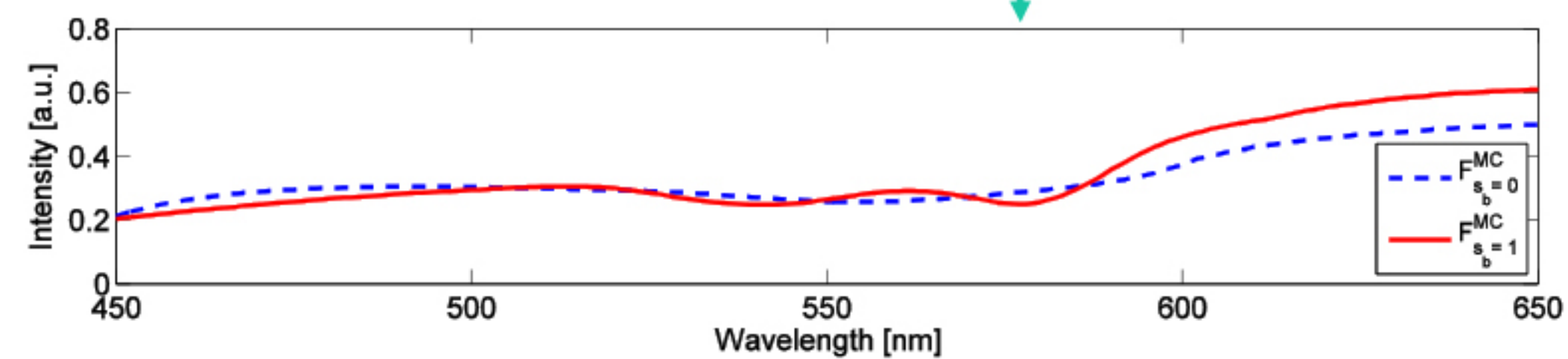
$$\begin{aligned} \mu_{a,b}(\lambda) = & (1 - s_b) \cdot c_b \cdot 0.15 \cdot \mu_{a,\text{Hb}}(\lambda) \\ & + s_b \cdot c_b \cdot 0.15 \cdot \mu_{a,\text{HbO}_2}(\lambda) \end{aligned}$$

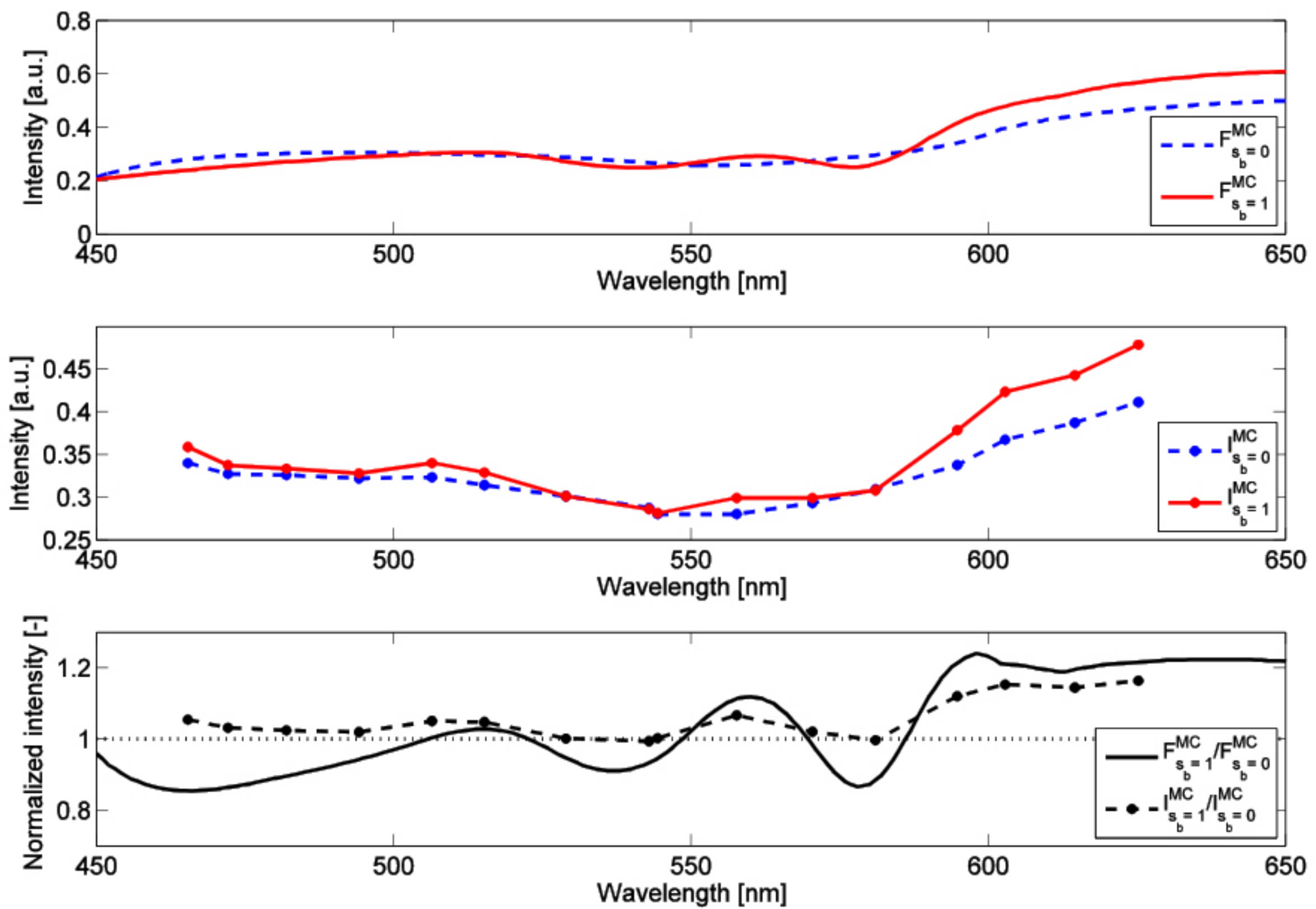


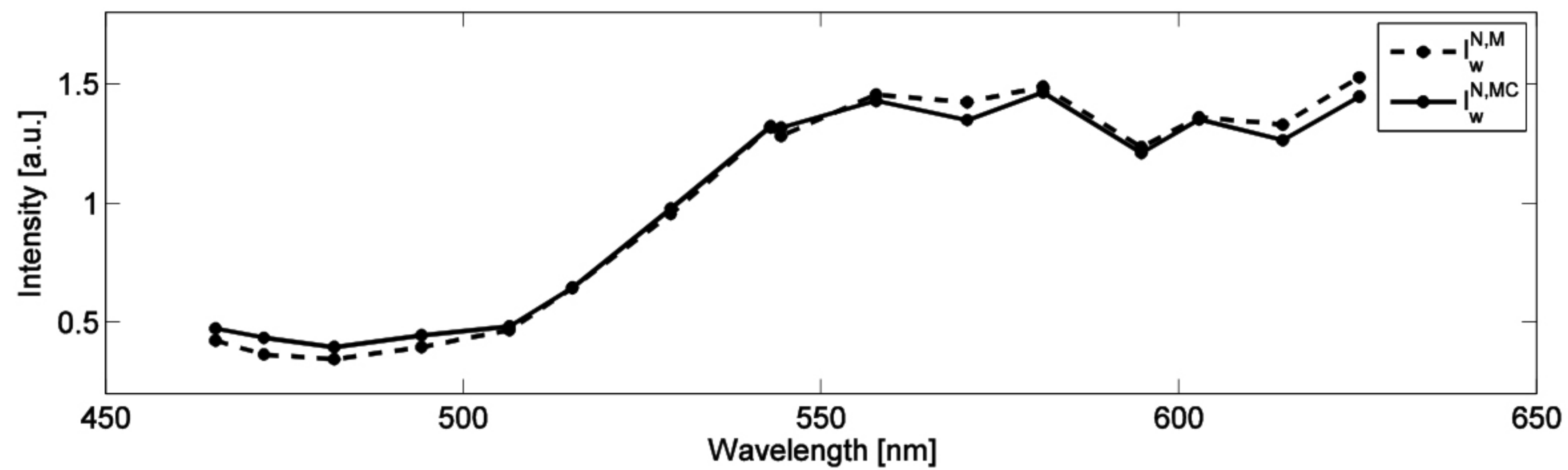
Modelling detected light



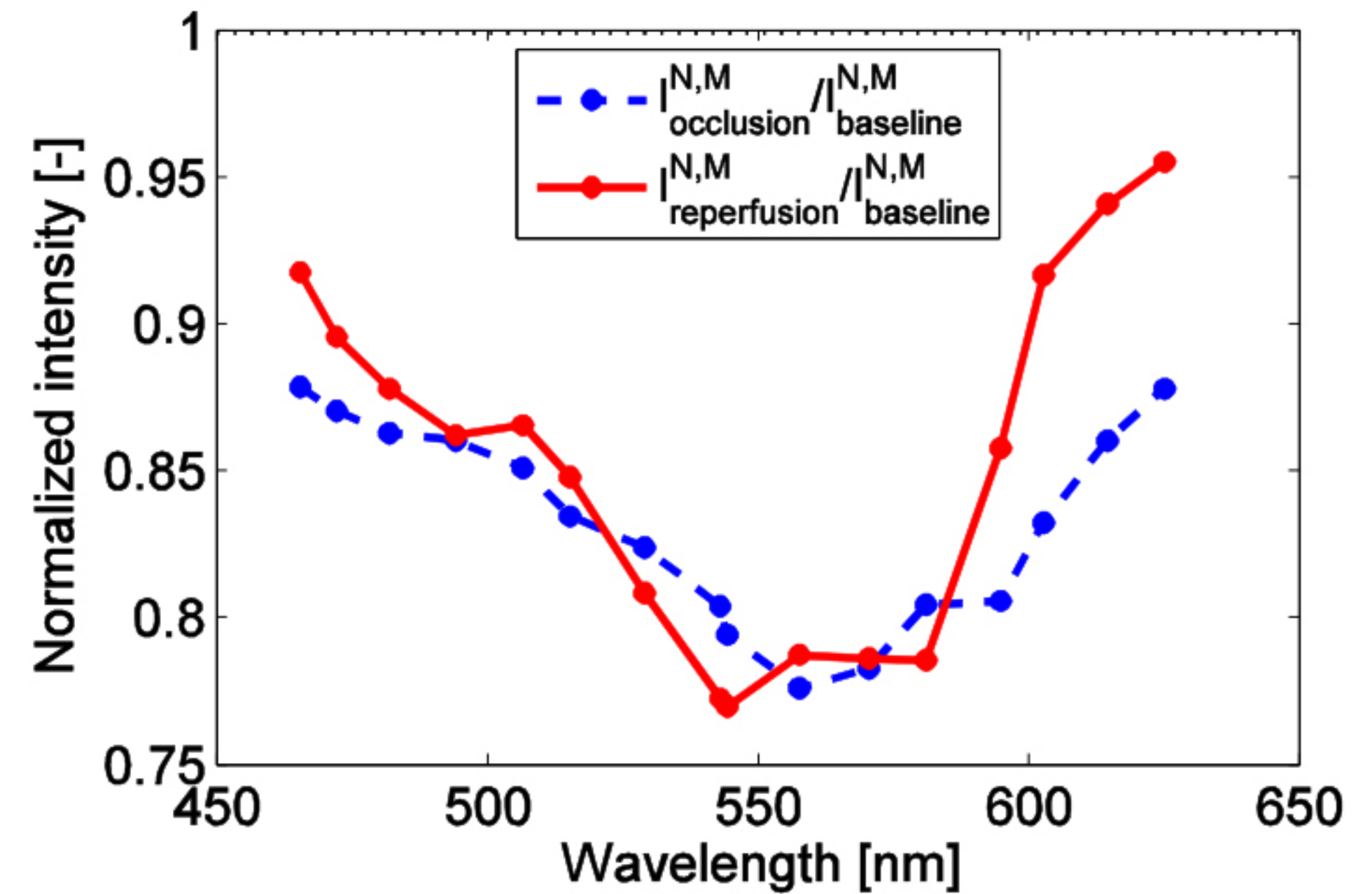
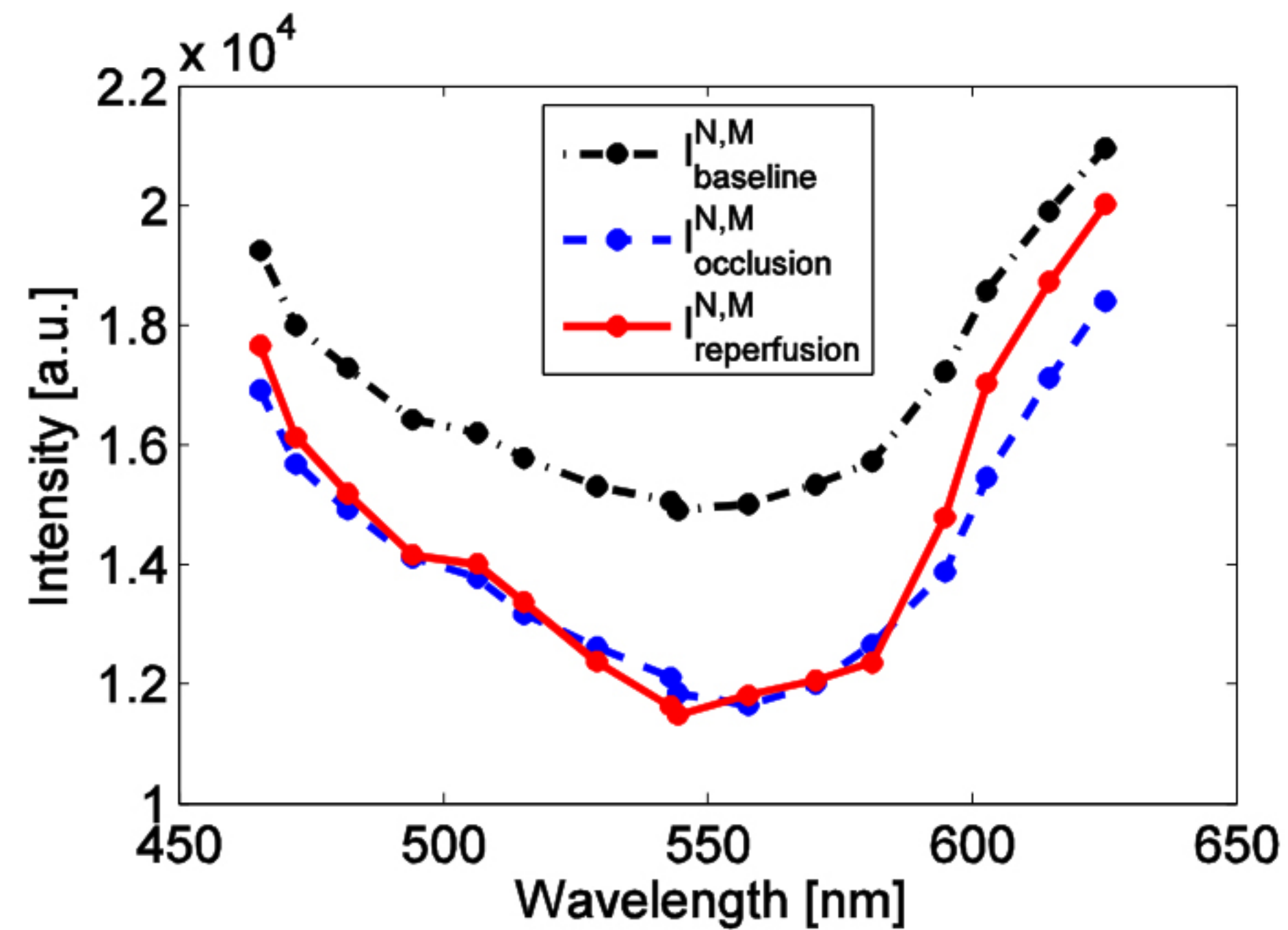
$$I_X^{MC}(n) = \sum_{\lambda} r_n(\lambda) \cdot L(\lambda) \cdot F_X^{MC}(\lambda)$$



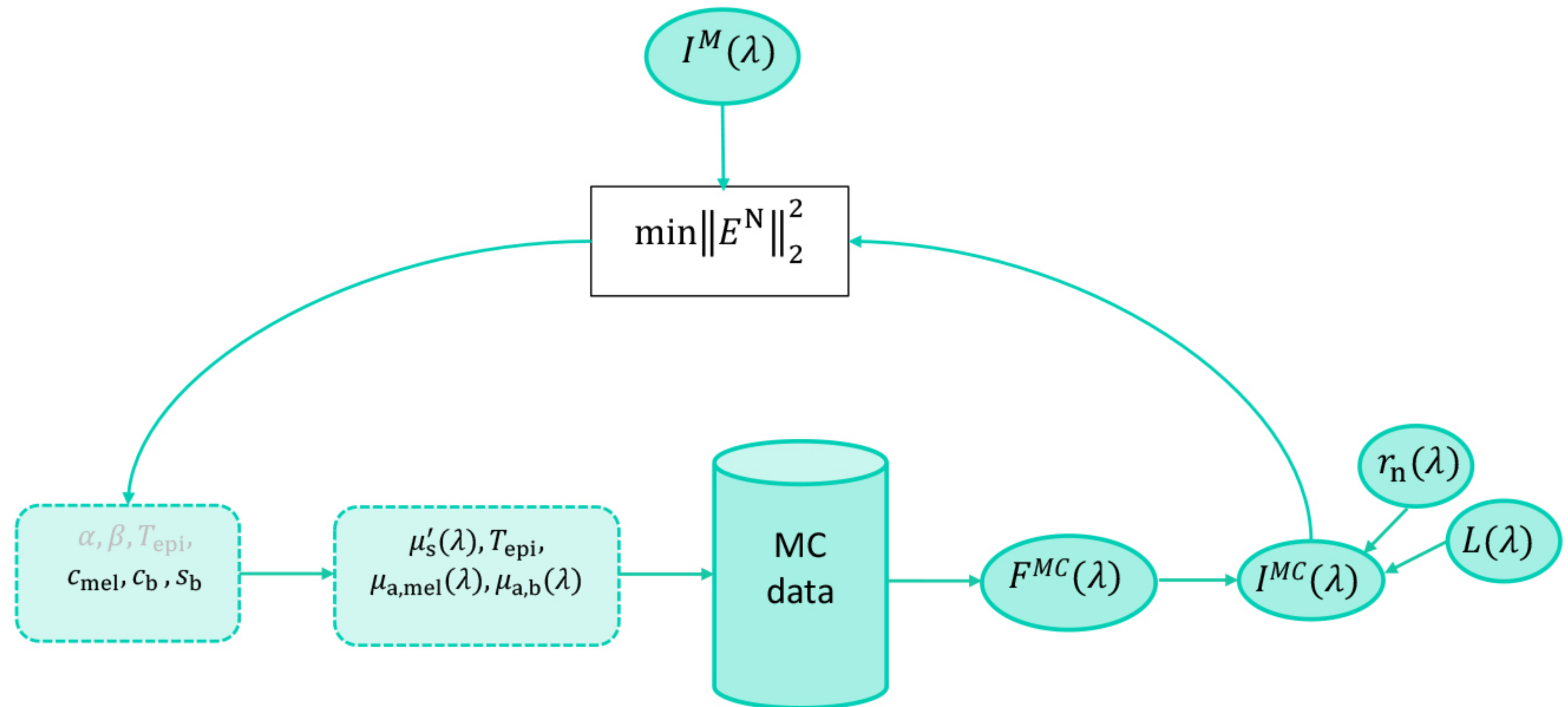




Measurement data



Inverse Monte Carlo algorithm



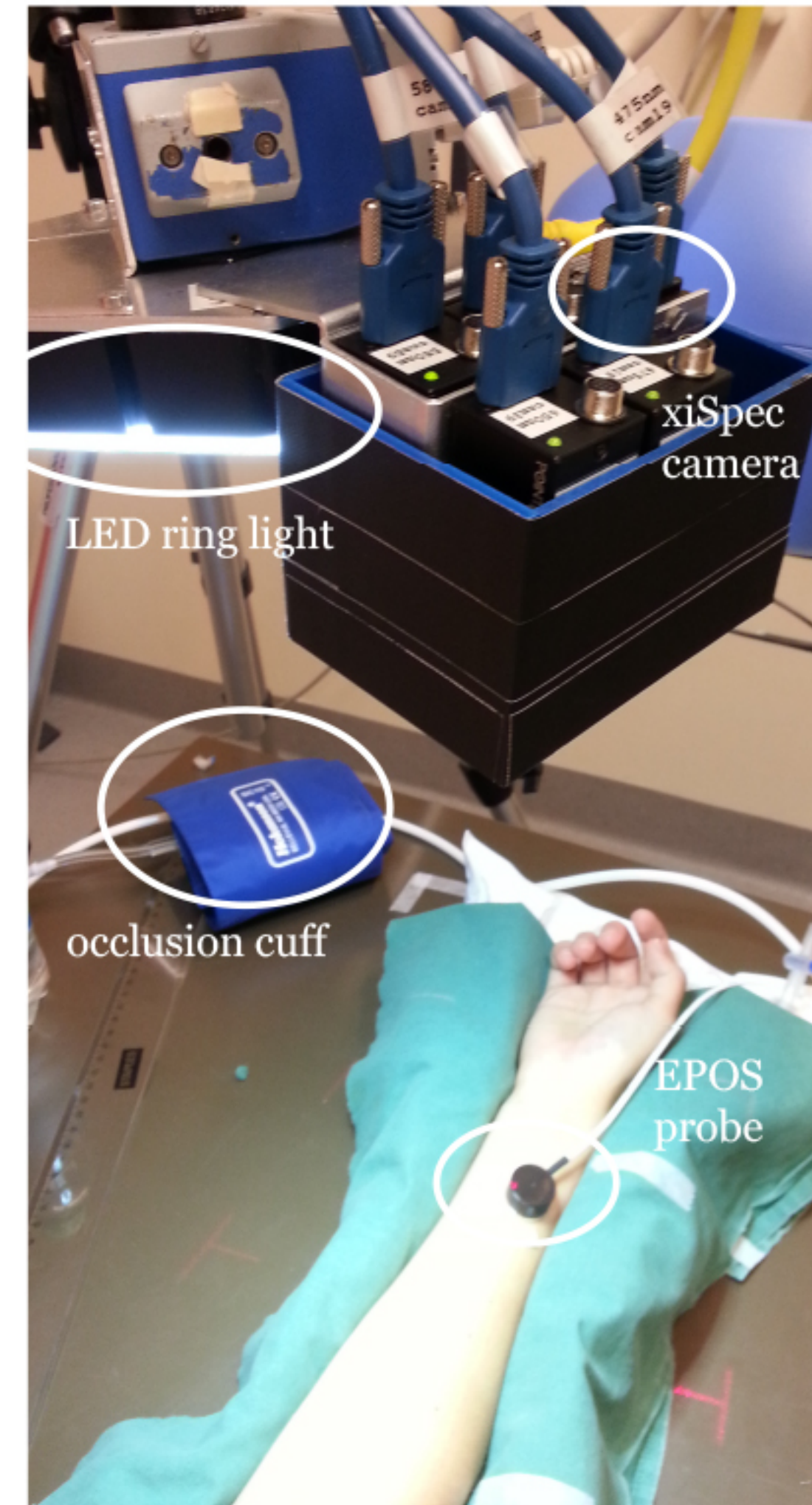
Penalty function

$$E^N = \begin{bmatrix} E_I^N(n) \\ 10 \cdot E_S^N \end{bmatrix}$$

- Spectral fit (chosen channels): $E_I^N(n) = \frac{I_x^{N,MC}(n)}{\langle I_x^{N,MC}(n) \rangle_n} / \frac{I_x^{N,M}(n)}{\langle I_x^{N,M}(n) \rangle_n} - 1$
- High saturation sensitivity: $E_S^N = \frac{I_x^N(557) + I_x^N(570)}{I_x^N(544) + I_x^N(580)}$
- Minimize penalty function: $\min \|E^N\|_2^2$

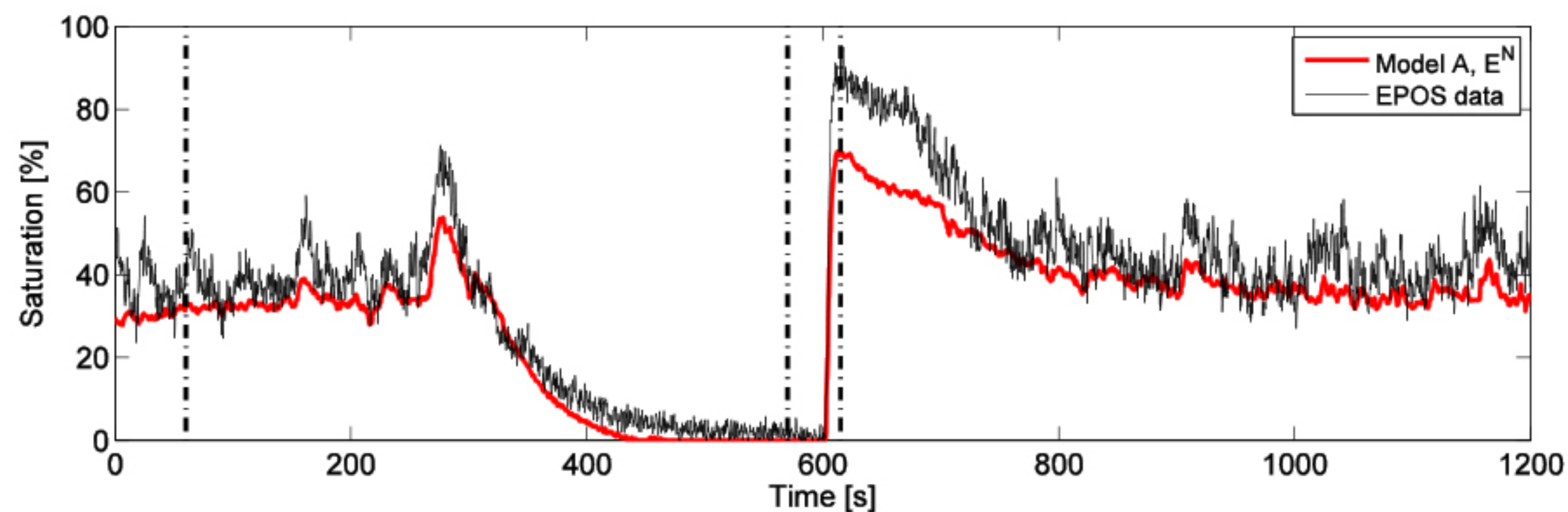
Provocation protocol

- Measurement setup
 - xiSpec camera
 - LED ring light
 - Probe DRS (EPOS) as reference
- Arterial occlusion of forearm
 - 5 min baseline
 - 5 min occlusion (250 mmHg)
 - 10 min after release

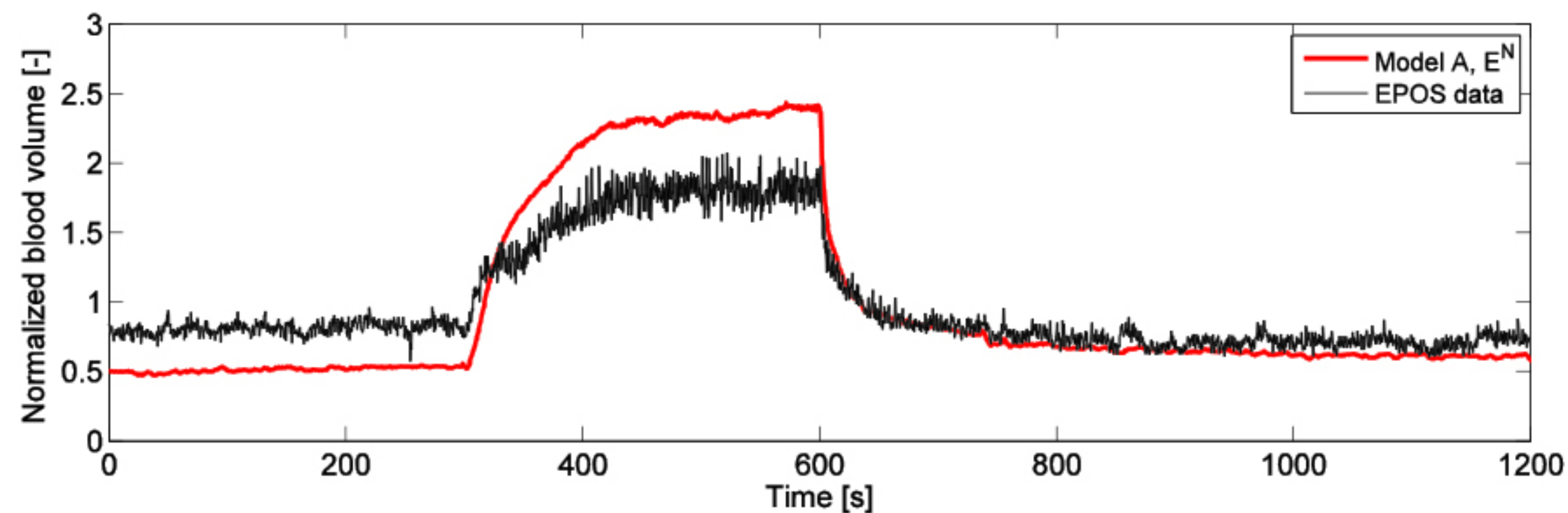


Results - temporal

Arterial occlusion
protocol:

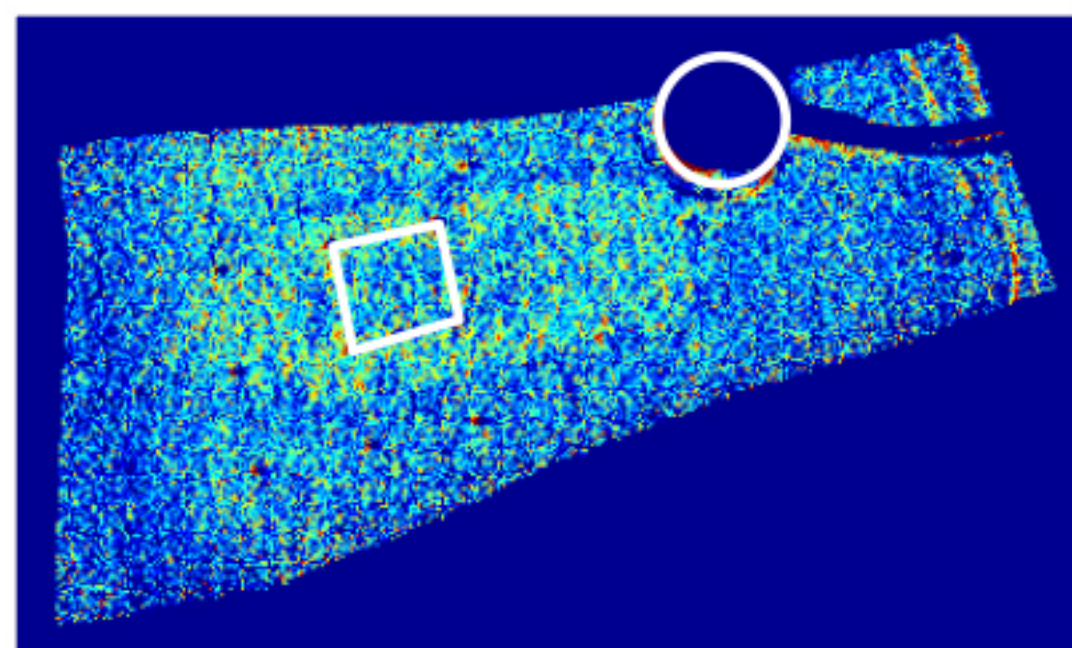


Venous occlusion
protocol:

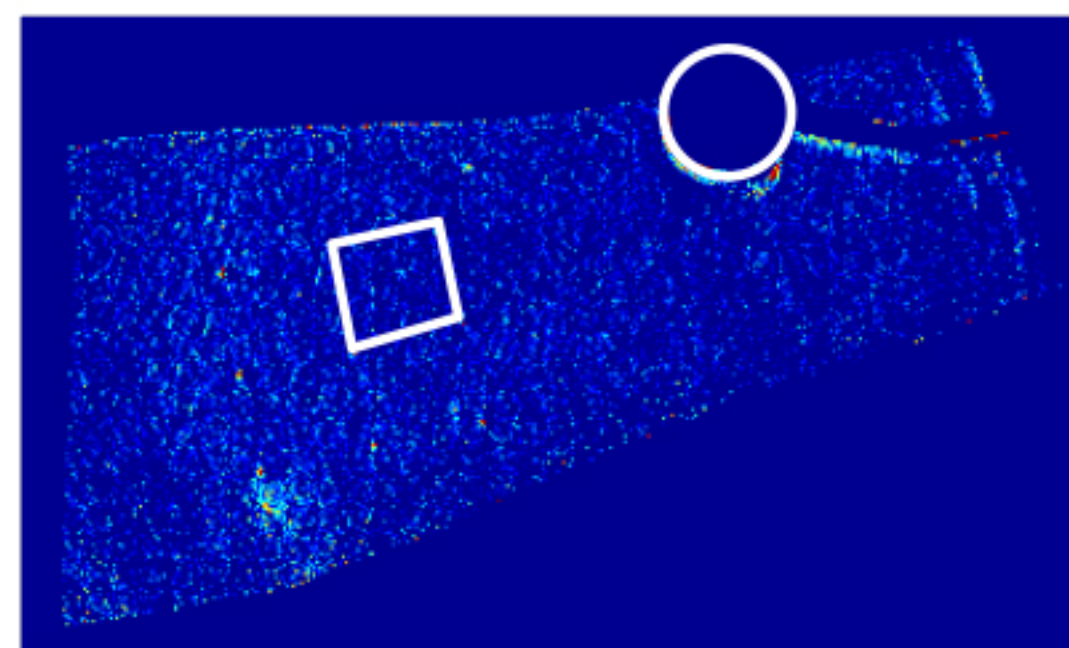


Results - spatial

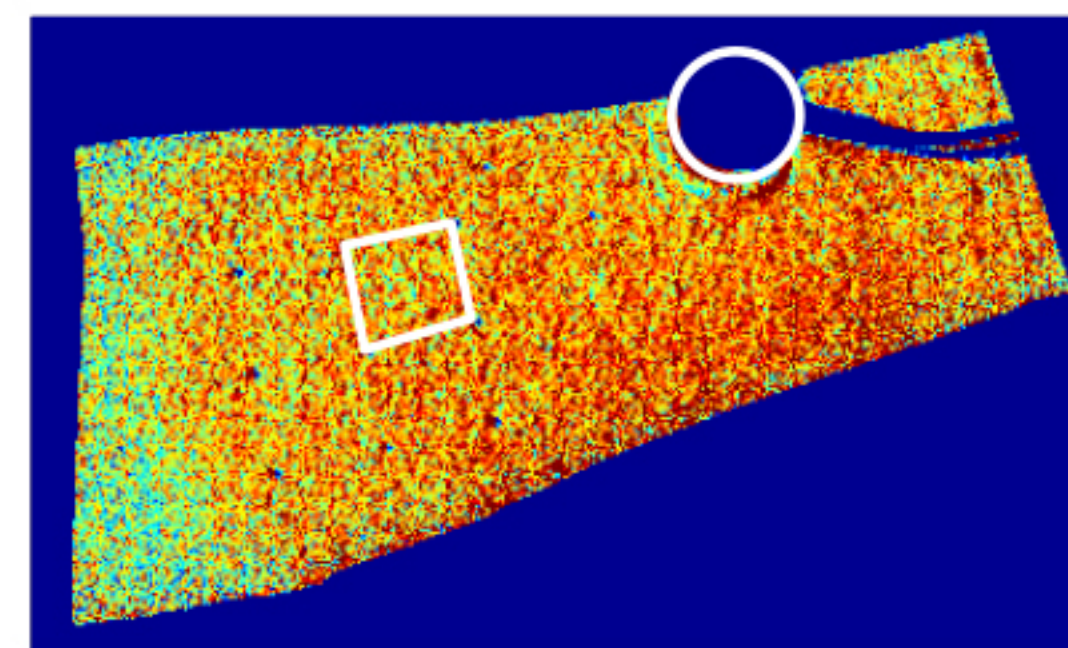
Arterial occlusion protocol, saturation:



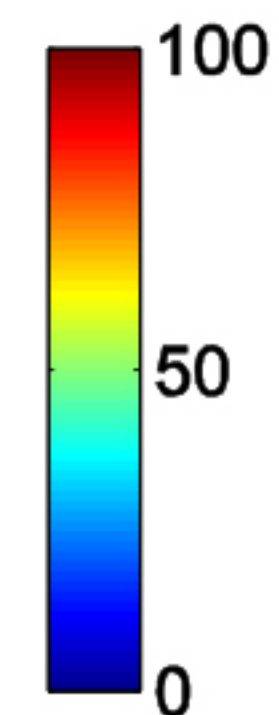
Baseline



Occlusion



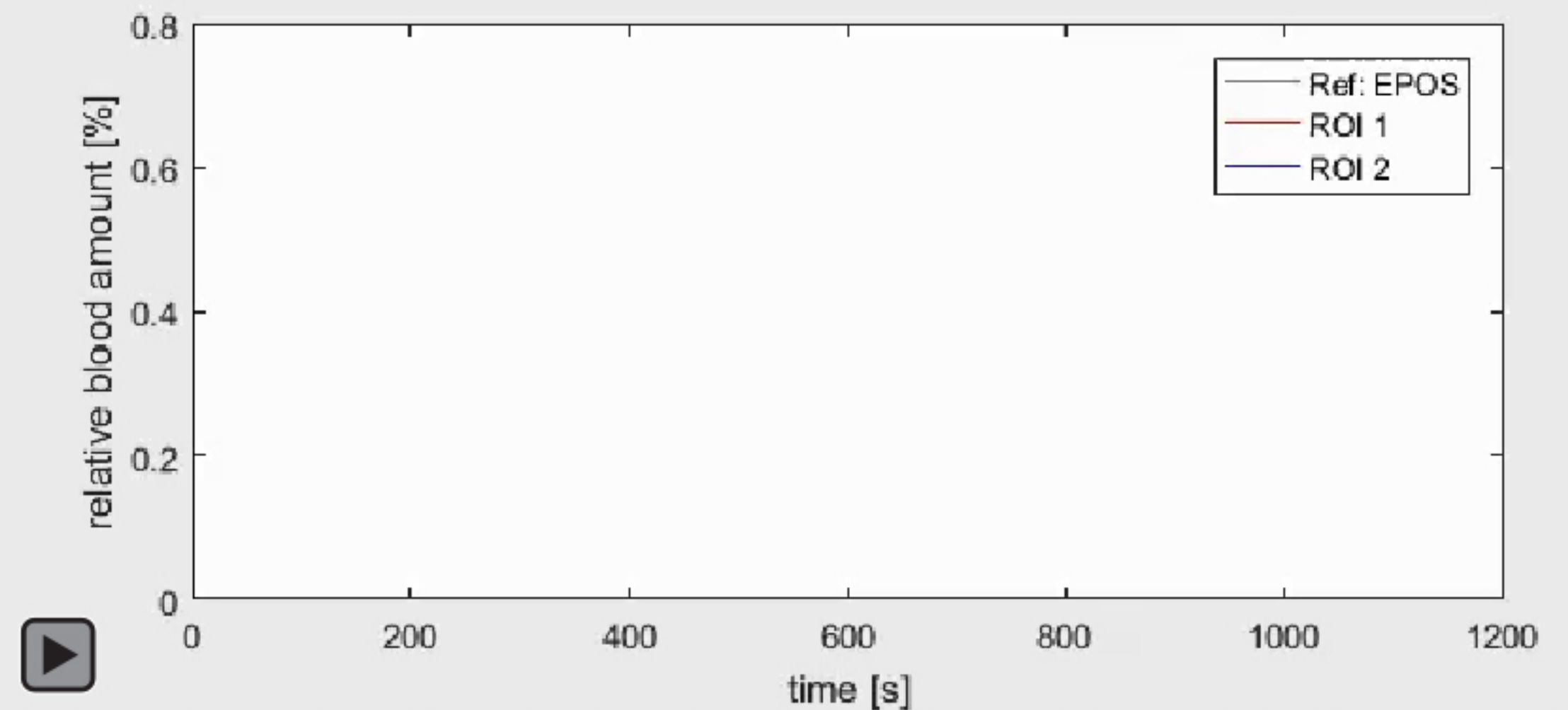
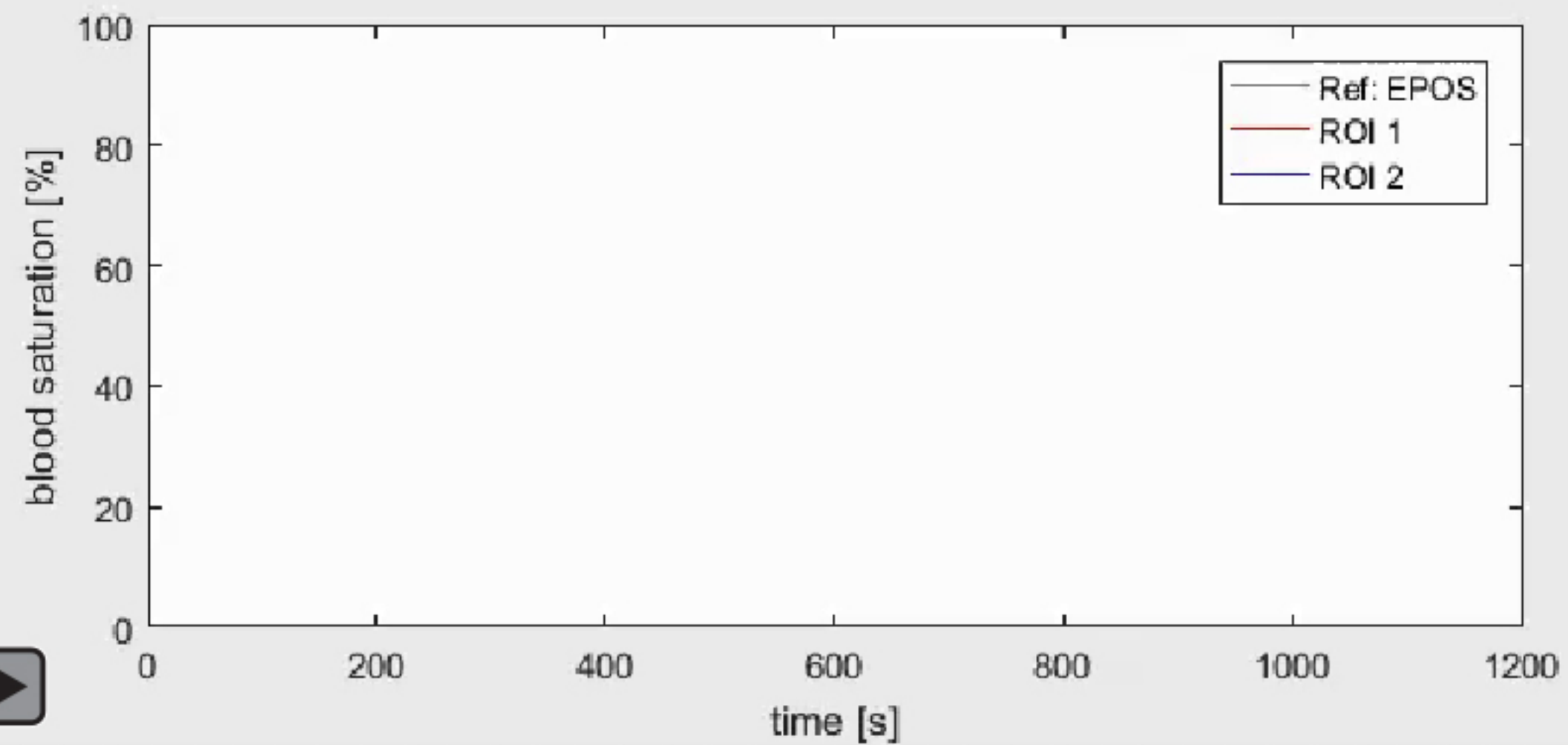
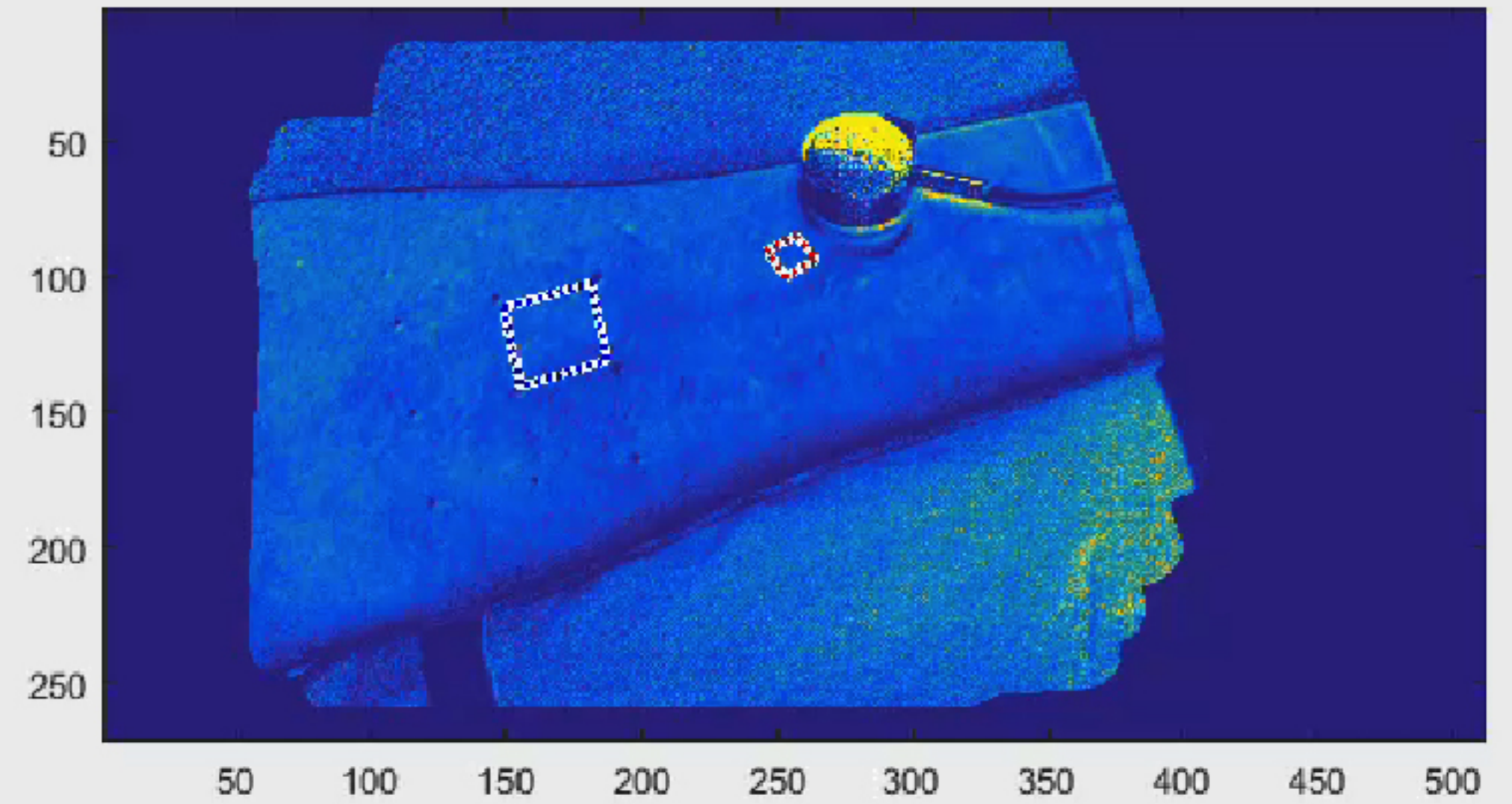
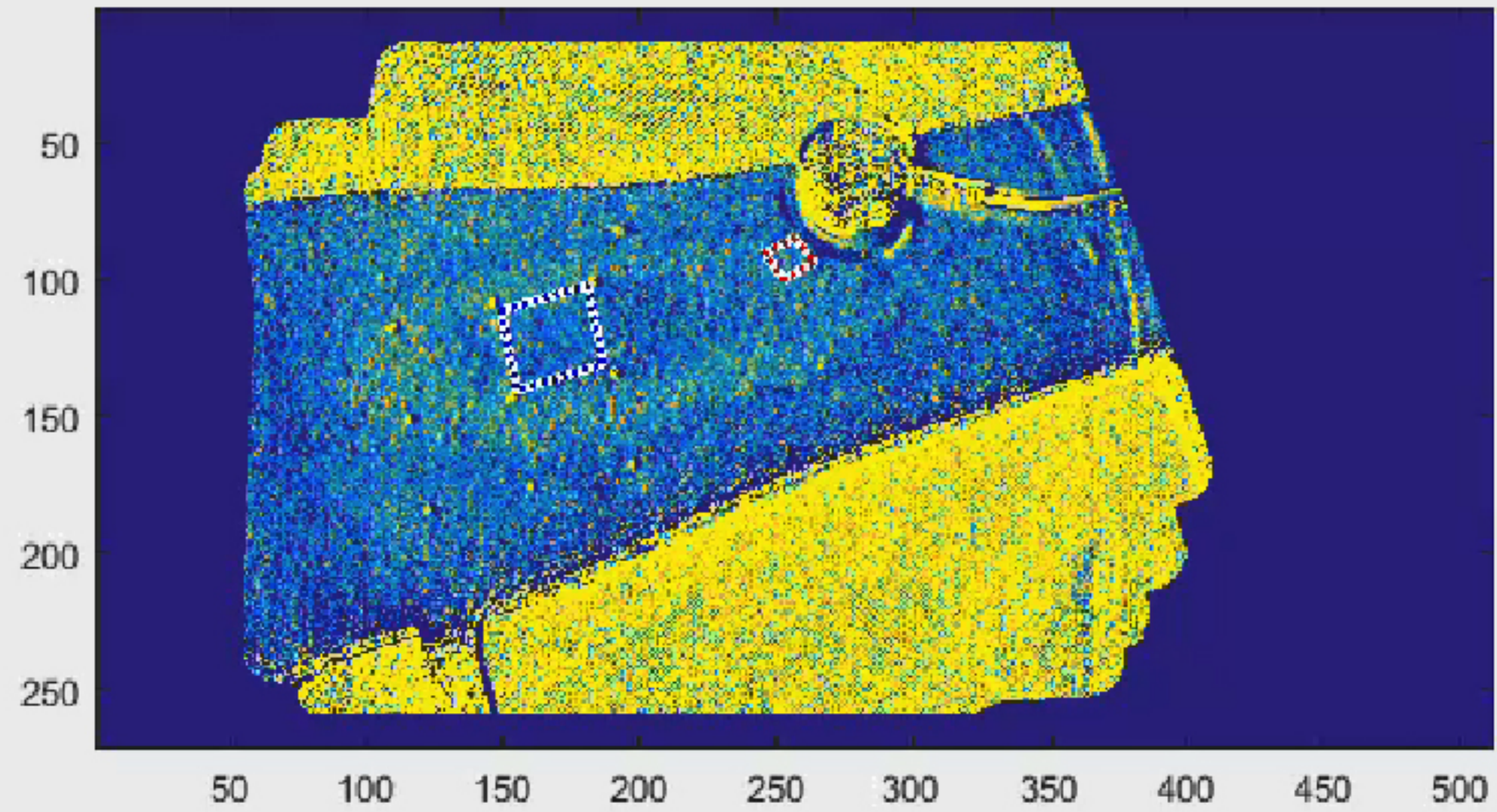
Reperfusion



Results – temporal and spatial

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Conclusions

- Oxygen saturation sensitive
- Blood concentration sensitive
- Visualize spatial and temporal
 - oxygen saturation and
 - blood concentration maps

Thank you for listening!

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